

Original Research Article

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## Application of Dental Implants Coated with Titanium Nitride: The Experimental Study with *Porphyromonas gingivalis* Infection

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### ABSTRACT

#### Keywords

Osseointegration, Peri-implant infection(s), *Porphyromonas gingivalis*, Infectious disease(s), Oral Rehabilitation.

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Dental implants have been effective for oral rehabilitation. Surface modification of implants is reportedly very important in achieving excellent osseointegration. In this study, a titanium nitride (TiN)-coated implant was evaluated using experimental infections in animals for use in dental implants. TiN-coated implants not only have optimal surface roughness to achieve osseointegration, but also have antimicrobial activity against *Porphyromonas gingivalis*, which is a pathogen in peri-implantitis. The present study demonstrated that TiN-coated implants showed less *P. gingivalis* surface adhesion and less bone resorption induced by *P. gingivalis*. In addition, the bone implant contact ratio of TiN-coated implants showed the highest percentage, with significant differences compared to machined, sandblasted, acid-etched, and radiofrequency magnetron sputter hydroxyapatite-coated surface modifications, even with *P. gingivalis* infection. This was the first report to demonstrate that TiN-coated implants were excellent for inducing osseointegration and inhibiting *P. gingivalis* infection using a simplified animal model.

### Introduction

The most common dental implant material is commercially-pure (cp) titanium. In recent years, modifications have been made to machined titanium implants with the aim of optimizing osseointegration (Lazzeera *et al.*, 1999; Lang *et al.*, 2009). These modifications to increase the speed and success of

osseointegration have included hydroxyapatite coatings, increasing surface roughness and surface free energy (Yoshinari *et al.*, 2002). Increasing surface roughness has been achieved with a titanium plasma-sprayed (TPS) surface, sand blasting, acid etching, and a sand-blasted large-grit acid-etched surface

(SLA) (Schroeder *et al.*, 1996). However, the amounts of bacterial adhesion and oral biofilm accumulation were reportedly accelerated by increasing surface roughness (Amoroso *et al.*, 2006; Teughels *et al.*, 2006). It was also difficult to remove these bacteria from the implant surface (Albouy *et al.*, 2010). Bacterial adhesion to biomaterials is an important factor in the pathogenesis of infection. Peri-implantitis is a common complication in implant therapy and is characterized by inflammatory lesions in peri-implant tissues and associated loss of supporting bone (Zitzmann and Berglundh, 2008). It is by definition an infectious disease and the inflammatory lesion in peri-implant tissues develops as a result of accumulation of bacteria on implant surfaces. Some studies reported that peri-implantitis occurs in 28% to 56% of subjects and at 12% to 43% of implant sites (Ferreira *et al.*, 2006; Roos-Jansaker *et al.*, 2006). The surface roughness and chemical composition of the implant surface are important in bacterial adhesion.

Titanium nitride (TiN) is a ceramic with great hardness (2,000 kg/mm<sup>2</sup>), high decomposition temperature (2,949°C), defect structure, i.e., deviation from stoichiometry, chemical stability at room temperature, superconductivity, and gold-yellow color (Toth 1971). TiN is mainly used as a coating to enhance other materials. TiN shows encouraging blood tolerability properties with hemolysis percentage near zero (Dion *et al.*, 1992). Therefore, TiN-coatings are used in cardiology for ventricular assist devices in patients with heart failure (Sin *et al.*, 2009) and for pacemaker leads (Schaldach *et al.*, 1989). In neurology, TiN-coated electrodes are used in chronically implanted devices for the treatment of spinal cord injury (Cogan, 2008). TiN-coating is also used in orthopedic implants, because of its excellent biological properties, such as the reduction of the release of cobalt-chromium-molybdenum ions, and

the aesthetic appeal of the “golden color” (Mezger and Creugers, 1992; Wisbey *et al.*, 1987).

It is important to consider TiN for use in implants because of reports about peri-implantitis. However, the utility of TiN-coated cp titanium dental implants using an experimental infection model has not been investigated in vivo. This study evaluated biological response in bone 2 weeks after placement of TiN-coated cp titanium implants using *Porphyromonas gingivalis*, a pathogen in peri-implantitis (Mombelli, 1997), in a simplified rabbit model.

## **Materials and Methods**

### **Animals**

This study was approved by the Animal Ethics and Research Committee of Health Sciences University of Hokkaido, Hokkaido, Japan (Approval No. 72). All animal experiments complied with the *Guidelines for the Care and Use of Laboratory Animals* of the University. A total 20 adult male Japanese white rabbits weighing approximately 2.5 kg (Hokudo Co, Sapporo, Japan) were used in this study. The rabbits were kept under a 24-hour light/dark cycle and had free access to drinking water at the Animal Experiment Center.

### **Dental Implants**

Forty threaded  $\mu$ -One HA implants (Yamahachi Dental MFG., Co., Aichi, Japan) ( $\phi$  3.3 mm, length 10.0 mm, identical in size to those in clinical use) were machined from a cp titanium rod (JIS TYPE 2) for use in this study. They were divided into 4 different groups based on surface modification: implant type M, machined; B, sandblasted and acid-etched; HA, radiofrequency magnetron sputter hydroxyapatite (HA)-coated (1-2  $\mu$ m);

TiN, TiN-coated (3.1  $\mu\text{m}$ ) using an arc ion plating system (AIP-S40, KOBELCO, Tokyo, Japan) for 90 min, 150 A, 30 V, with  $\text{N}_2$  partial pressure of 4 Pa.

### Surface Topography and Roughness

Scanning electron microscopy (SEM) (SSX-550, Shimazu, Japan) was used for an overall picture of the surface topography of implants with each surface modification. SEM micrographs were taken at the surface between the 2<sup>nd</sup> and 3<sup>rd</sup> threads of the implant at a magnification of 1,000 $\times$ .

Quantitative characterization of the surface topography and roughness was carried out by 3-dimensional (3D) laser microscopy (LEXT OLS4000, Olympus, Tokyo). The roughness (Ra) of each implant was determined to set the X and Y horizontal and vertical axes of the implants. One sample of each preparation type was analyzed at randomly chosen areas (258  $\times$  258  $\mu\text{m}^2$ , cutoff value: 8  $\mu\text{m}$ ) on the flat part at the bottom of the implant.

### Bacterial Strain and Culture Conditions

*P. gingivalis* ATCC 33277<sup>T</sup> and *Prevotella intermedia* ATCC 25611<sup>T</sup> were used in this study. Culture was on Bacto<sup>TM</sup> Brain Heart Infusion (BHI, Difco Laboratories, BD) supplemented with 5% (volume/volume) defibrinated sheep blood (BHI agar), hemin (10  $\mu\text{g}/\text{mL}$ ), and menadione (5  $\mu\text{g}/\text{mL}$ ) under anaerobic conditions ( $\text{N}_2:\text{CO}_2:\text{H}_2 = 80\%:10\%:10\%$ ) at 37°C for 5 days. Bacterial cells of *P. gingivalis* colonies were collected with a cotton wool stick, washed, and suspended in phosphate-buffered saline (PBS) (pH 7.2) to a turbidity equivalent to  $\text{OD}_{660} = 10.0$  ( $1.5 \times 10^9$  cells/mL), and also suspended in BHI broth supplemented with hemin and menadione to a turbidity equivalent to  $\text{OD}_{660} = 0.1$  ( $1.5 \times 10^7$  cells/mL) with a spectrophotometer.

### Bacterial Adherence Test

Bacterial adherence to the M-, B-, HA-, and TiN-coated disks,  $\phi$  10 mm, thickness 1 mm, was examined for *P. gingivalis*. Each of the 4 kinds of disks were placed in a 24-well plate and incubated with 1 mL of bacterial suspension in BHI broth ( $\text{OD}_{660} = 0.1$ ) for 2 weeks under anaerobic conditions at 37°C. Medium replacements were carried out every 5 days in 2 weeks. After incubation, the disks were transferred to 1 mL PBS and vortexed for 2 min to roughly remove bacterial cells from the disk surface. The disks were then transferred to 1 mL PBS again and sonicated for 30 s to completely remove the bacterial cells. After the disks were removed, the PBS-containing bacterial cells were mixed and centrifuged (8,500 rpm, 4°C, 15 min). The precipitated bacterial cells were suspended to 1 mL with PBS.

A 100- $\mu\text{L}$  suspension was transferred to 900  $\mu\text{L}$  of PBS, and serially diluted 10-fold with sterile saline from  $10^{-3}$  to  $10^{-7}$ . A 100- $\mu\text{L}$  aliquot of diluted solution was placed on BHI blood agar plates, spread evenly with beads, and cultured for 5 days under anaerobic conditions at 37°C. After incubation, colony-forming units (CFU) were counted.

The entire genomic DNA was extracted by InstaGene Matrix Kit (Bio-Rad) according to the manufacturer's instructions from the residual 900  $\mu\text{L}$  of the precipitated bacterial cell suspension to measure the total amount of bacteria. DNA concentrations were determined by measuring absorption at  $\text{OD}_{260}$ . The results were analyzed from 3 independent experiments performed in triplicate.

### Surgical Procedure and *P. gingivalis* Provision

Dental implant placement was performed under general anesthesia using intravenous

pentobarbital sodium 16.2 mg/kg (Somnopenyl Kyoritsu seiyaku Co., Tokyo, Japan) into the ear vein. After preparing the surgical field, local anesthesia was performed using lidocaine HCl containing 2% epinephrine 1.8 mg/kg (Xylestesin A injection solution, ESPE, Germany). The procedure of implant placement was previously described (Nakanishi *et al.*, 2011).

After implant placement, silk threads were twisted 4 times on the abutment-implant junction. *P. gingivalis* suspension 15  $\mu$ l (OD<sub>660</sub> = 10.0) was applied to silk threads on the left side as the infection model, *P. g* (+); 15  $\mu$ l of PBS was applied to the silk threads on the right side as the control, *P. g* (-). Then, one eco-tube (4  $\times$  6 mm) and one silicone tube (5  $\times$  7 mm) were used to prevent the silk threads from falling out, followed by suturing of the periosteum and skin. No antimicrobial agents were used. The experiments were repeated 5 times for each type of implant (M, HA, B, and TiN). The experimental period lasted for 2 weeks, as in a previous report (Ochi *et al.*, 2003).

### **Bacterial Sampling**

After the rabbit was sacrificed with a pentobarbital sodium overdose, bacterial samples were collected using sterile paper points (ISO #35) from the sulcus around the implant. Samples were also collected from the control side. The samples were immediately placed in 1 mL of sterile PBS, vortexed for 2 min, and homogenized 100 times to disperse bacterial cells from the paper points. The bacterial cells from the paper points were collected by centrifugation.

### **DNA Extraction and Detection of *P. gingivalis* by Polymerase Chain Reaction (PCR)**

Genomic DNA was extracted from individual samples using the InstaGene Matrix Kit. DNA

concentrations were determined by measuring absorption at OD<sub>260</sub>.

For detection of all bacteria, a 16S rDNA universal primer set (forward: 5'-GAGAGTTTGATYMTGGCTCAG-3', reverse: 5'-GAAGGAGGTGWTCCARCCGCA-3') (Paster *et al.* 2001) was used. A specific primer set (forward: 5'-AGGCAGC TTGCCATACTGCG-3, reverse: 5'-ACTG T TAGCAACTACCGATGT-3') (Bogen and Slots 1999) was also used to detect *P. gingivalis*. PCR was performed according to previous reports (Paster *et al.*, 2001; Bogen and Slots, 1999).

*P. intermedia*, which is genetically related to *P. gingivalis*, was used as a negative control. PCR products were applied to 1.5% agarose gels. Following electrophoresis, gels were stained with SYBR<sup>®</sup> Safe DNA gel stain (Invitrogen).

### **Sample Removal and Specimen Preparation**

After bacterial sampling, surrounding bone including the implant in both sides of the femurs was removed. The specimen preparation procedure was previously described by Nakanishi *et al.*, (2011).

### **Observation by Contact Microradiography (CMR) and Measurement of Bone Implant Contact Ratio (BIC)**

Pictures of samples with a thickness of 120  $\mu$ m were taken using a soft X-ray generation device (Sofron Model BSTI 1505CX<sup>®</sup> Souken Laboratory, Tokyo, Japan). Bone resorption area (mm<sup>2</sup>), bone resorption depth (mm), and maximum bone resorption width (mm) around the implant were measured after magnification correction, shown in Fig. 1(a).

BIC was measured by using sections stained with basic fuchsin and methylene blue.

Measurements were separately conducted for upside BIC (from the top of the implant to the 3<sup>rd</sup> thread) and downside BIC (from the 4<sup>th</sup> thread to the bottom of the implant). Computer analysis with NIH Image<sup>®</sup> 1.61 (National Institutes of Health, Bethesda, MD, USA) was performed with image analysis software. BIC was calculated as the ratio of the contact length of the implant and newly-formed bone adjacent to the implant as peripheral length (contact length/implant peripheral length of implant and newly formed bone)  $\times$  100%.

### Statistical Analysis

Statistical significance was determined using Tukey's analysis after one-way analysis of variance (ANOVA) with SPSS<sup>®</sup> Statistics 22 (IBM SPSS Inc., Chicago, IL, USA). A p-value of <0.05 was considered statistically significant.

## Results and Discussion

### Laboratory Animals

No anomalous variation or abnormal findings in rabbits infected with *P. gingivalis* were observed for the 2 weeks of the experiment.

After 2 weeks, inflammation in the affected area was observed in all *P. g* (+) groups. Specifically, tumefaction and reddening in all *P. g* (+) groups, and drainage in *P. g* (+) HA and B groups, were observed. No inflammation in the affected area was detected in any of the *P. g* (-) groups (data not shown).

### Surface Topography and Roughness

The surface topography of M-, B-, HA-, and TiN-coated implants is shown in Fig. 2(a) SEM images. M had the typical topography of machined samples: flat and smooth, with machining grooves. B, HA, and TiN had

many surface concavities and convexities, but no drastic vertical interval in the 3D laser microscopy image, Fig. 2(b). The surface roughness (Ra) was calculated according to the 3D laser microscopy image. The results of Ra (X axis, Y axis) ( $\mu\text{m}$ ) were shown in Table 1. According to the Ra measurement, M clearly showed less roughness than B, HA, and TiN. Furthermore, HA showed less roughness than B and TiN.

### Bacterial Adherence Test

The amount of bacterial adherence to the M-, B-, HA-, and TiN-coated disks was determined by CFU and the total amount of DNA. The mean CFU values (CFU/mL) and the amounts of DNA (ng) were shown in Table 1. These data indicated that cells of *P. gingivalis* did not tend to adhere to TiN, but the results showed no significant difference.

### Detection of *P. gingivalis*

No PCR products were detected in any *P. g* (-)-affected areas by analysis using the 16S rDNA universal primer set. PCR products were confirmed in all but the *P. g* (+)-affected TiN areas using the same primer set (data not shown).

The results of PCR analysis with the specific primer set for *P. gingivalis* are shown in Fig. 3. This analysis demonstrated that *P. intermedia* could not manufacture PCR products with the specific primers (Fig. 3, lane 2). This result indicated the specificity and utility of the specific primer set for *P. gingivalis*. PCR products were only confirmed in *P. g* (+)-affected areas of M, B, and HA (Fig. 3, lanes 3, 4, and 6). However, there were fewer PCR products from *P. g* (+)-affected areas of M than those of B and HA. No PCR products were confirmed in *P. g* (+)-affected areas of TiN, or in any *P. g* (-)-affected areas (Fig. 3, lanes 5, 7, 8, 9, and 10).



### **CMR Images and Measurement of Bone Resorption Area, Depth, and Width around the Implant**

CMR images of M, B, HA, and TiN with *P. g* (-) and *P. g* (+) are shown in Fig. 1(b). In the upper stages, there was no visible bone resorption with any type of implant in *P. g* (-) groups, but in lower stages, visible bone resorption was observed in B and HA of the *P. g* (+) groups.

Bone resorption area (mm<sup>2</sup>), bone resorption depth (mm), and the maximum of bone resorption width (mm) around the implant were measured in detail and shown in Table 1. In the *P. g* (-) group, there were no significant differences.

In contrast, in the *P. g* (+) group, there were significant differences between HA and M, B, and TiN as shown in Fig 1(c). In addition, the mean values of bone resorption depths and widths showed significant differences in both depths and widths between M and HA, between HA and TiN, and between M and B, shown in Fig. 1(d), (e).

### **Histologic Observation and Measurement of BIC**

Fig. 4(a), (b) shows the results of images stained with basic fuchsin and methylene blue. Existing bone was pink with basic fuchsin and methylene blue dyes, and bone-like tissue was purplish-red. Although newly-formed immature bone stained purplish-red was observed for all types of implant surfaces, the amounts in the *P. g* (+) group, shown in Fig. 4(b), were less than those in the *P. g* (-) group, shown in Fig 4(a).

BIC (%) was measured 2 weeks after the implant operation. The mean values of upside BIC in the *P. g* (-) groups and *P. g* (+) group were shown in Table 1. There was a

significant difference between TiN and M, B, and HA, shown in Fig. 4(c). The mean values of downside BIC in the *P. g* (-) group and *P. g* (+) group were shown in Table 1. There was a significant difference between M and B, HA, and TiN, shown in Fig. 4(d), (e).

A series of animal studies concluded that osseointegration can occur using an implant with a rough surface, but is difficult to achieve using a once-contaminated, machined (smooth) implant surface (Persson *et al.*, 2001).

In this study, B and TiN showed greater surface roughness than M and HA, suggesting that TiN was suitable as an implant surface to achieve osseointegration. In other studies, some regions of the TiN-coated implants showed no bone opposition at 4 weeks, but after 24 weeks, some specimens showed direct bone opposition in dog femurs (Hayashi *et al.*, 1989). The affinity of bone for the implant index of TiN-coated stainless steel was comparable to that of alumina, but not significantly better than uncoated stainless steel (Hayashi *et al.*, 1989). TiN-coated Ti6Al4V rods were implanted in rat femurs and showed biocompatibility and bone-bonding properties similar to uncoated Ti6Al4V rods (Sovak *et al.*, 2000). Relative bone area and BIC of TiN-coated cp titanium threaded implants in rabbits were similar to TiO<sub>2</sub>-coated cp titanium (Larsson *et al.*, 2013).

In this study, the amounts of bone resorption and BIC with *P. gingivalis* infection were evaluated by using 4 kinds of implant surfaces including TiN-coating. In the CMR images, HA in the *P. g* (+) group showed high amounts of bone resorption, whereas M and TiN in the *P. g* (+) group showed low resorption. Henry *et al.*, (1994) reported that HA implants more easily caused bone resorption with peri-implantitis than titanium

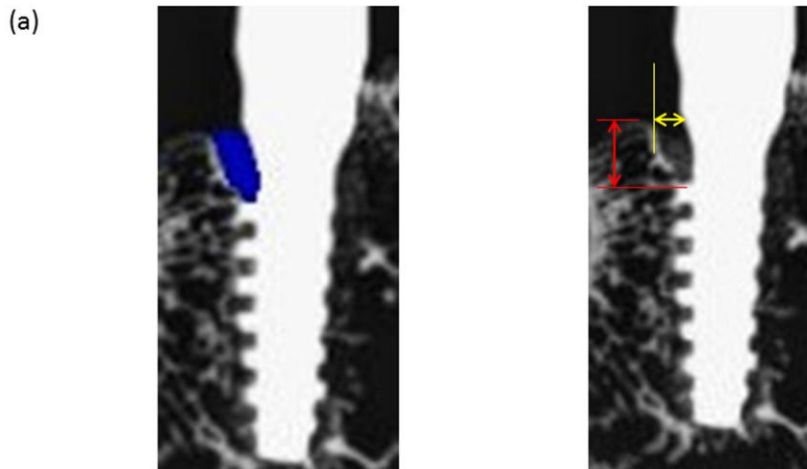
implants. On the other hand, M reportedly caused bone resorption less easily because the machined (smooth) surface made it difficult for *P. gingivalis* to adhere. In addition, PCR results showed that *P. gingivalis* was not detected on TiN, and was detected less on M than on B and HA. However, in the bacterial adherence test results, only TiN did not show

good adherence by *P. gingivalis*. Therefore, the results of our study partly support some reports (Henry *et al.*, 1994; Persson *et al.*, 2001), and suggest that the results of differences for M occurred in the in vitro and in vivo studies because of totally different conditions.

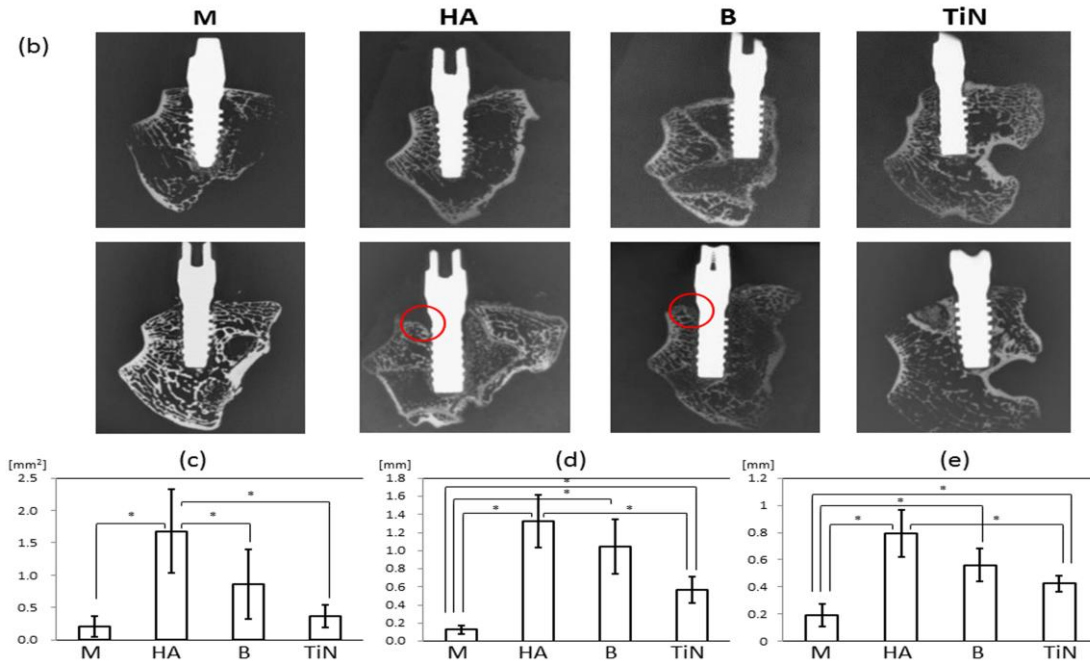
**Table.1** Summary of results in this study

Surface Modification	Surface Topography and Roughness		Bacterial Adherence Test		Measurement from CMR Images						BIC			
	Ra ( $\mu\text{m}$ )		CFU (mL)	DNA (ng)	<i>P. g</i> (-)			<i>P. g</i> (+)			<i>P. g</i> (-) [%]		<i>P. g</i> (+) [%]	
	X axis	Y axis			Bone resorption area [mm <sup>2</sup> ]	Depth [mm]	Width [mm]	Bone resorption area [mm <sup>2</sup> ]	Depth [mm]	Width [mm]	Upside	Downside	Upside	Downside
M	0.024 $\pm$ 0.005	0.016 $\pm$ 0.002	1.02E + 08	504.7	0.21	0.22	0.41	0.21	0.13	0.19	65.6	50.7	54.3	56.0
B	0.207 $\pm$ 0.018	0.259 $\pm$ 0.011	9.76E + 07	549.4	0.22	0.23	0.23	0.86	1.05	0.54	80.6	80.5	56.0	74.4
HA	0.191 $\pm$ 0.015	0.202 $\pm$ 0.019	1.01E + 08	575.7	0.10	0.20	0.21	1.68	1.33	0.80	78.8	83.5	53.8	76.9
TiN	0.237 $\pm$ 0.038	0.269 $\pm$ 0.028	5.66E + 07	445.7	0.13	0.42	0.21	0.36	0.57	0.36	77.1	75	77.3	70.1

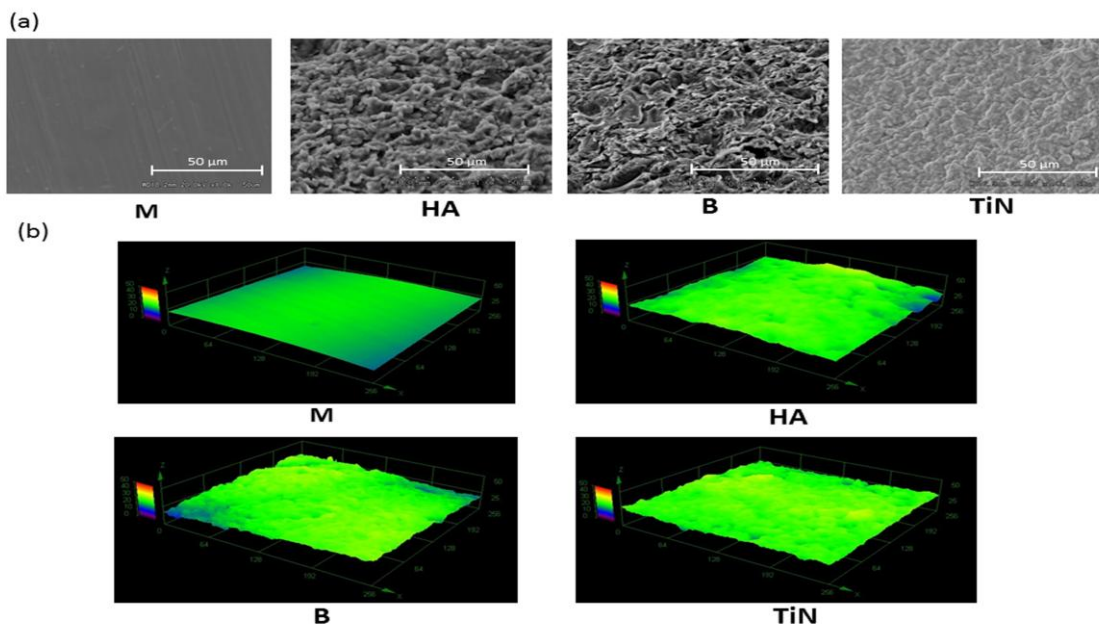
**Fig 1a** The results of measurement of bone resorption; blue: bone resorption area, red arrow: bone resorption depth, yellow arrow: bone resorption width



**Fig 1b** CMR images of M, B, HA, and TiN, with *P. g* (-) (upper stage) and *P. g* (+) (lower stage); red circles show visible bone resorption, (c): The results of measurement of bone resorption areas (mm<sup>2</sup>), \*P < 0.05, (d): The results of measurement of bone resorption depths (mm), \*P < 0.05, (e): The results of measurement of bone resorption widths (mm), \*P < 0.05.

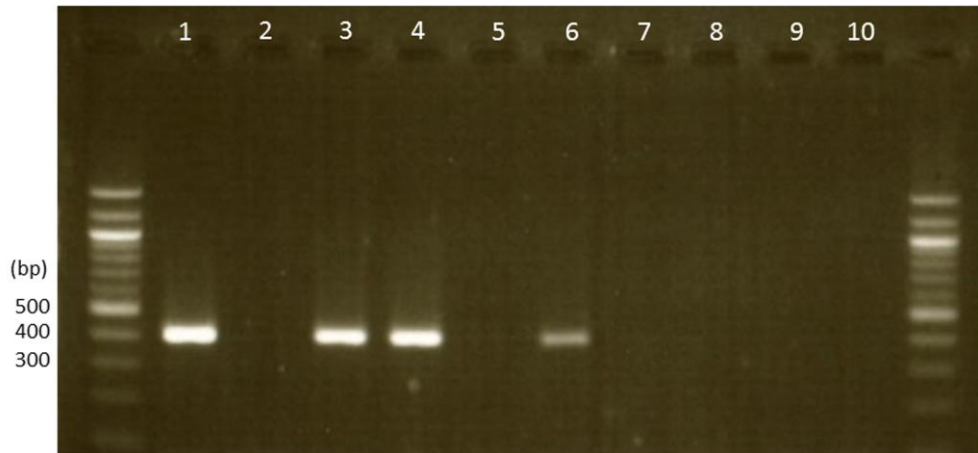


**Fig 2a** Scanning electron microscopy (SEM) images (1,000× magnification) of M, B, HA, and TiN, (b): 3D laser microscopy images (50× magnification) of M, B, HA, and TiN.

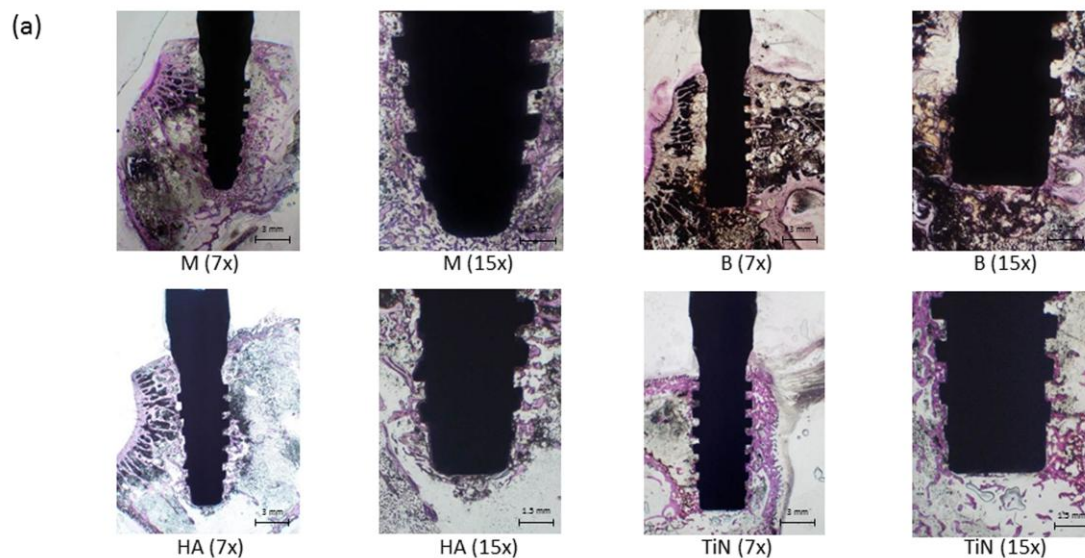


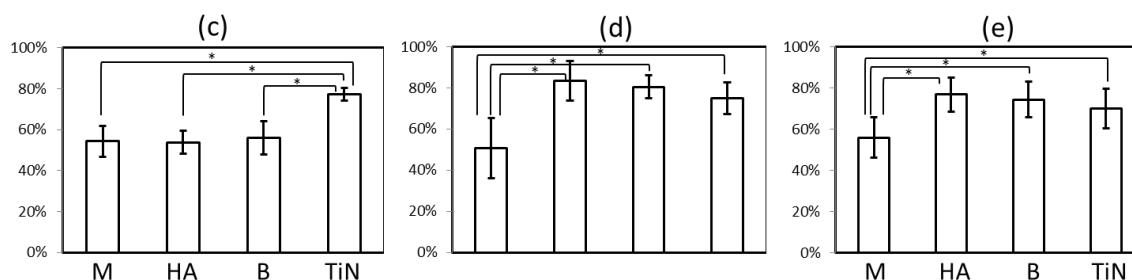
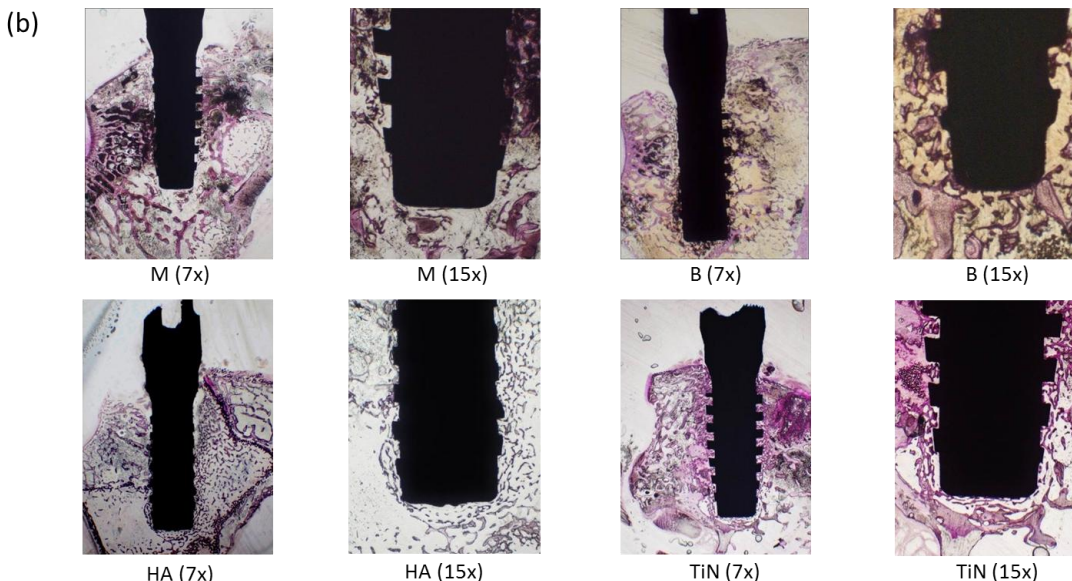


**Fig 3** The results of PCR electrophoresis with specific primer for *P. gingivalis*: lane 1, *P. gingivalis* ATCC 33277T as positive control; lane 2, *P. intermedia* ATCC 25611T; lane 3, HA in the *P. g* (+) group; lane 4, B in the *P. g* (+) group; lane 5, TiN in the *P. g* (+) group; lane 6, M in the *P. g* (+) group; lane 7, HA in the *P. g* (-) group; lane 8, B in the *P. g* (-) group; lane 9, TiN in the *P. g* (-) group; lane 10, M in the *P. g* (-) group.



**Fig 4a** Images of M, B, HA, and TiN, with *P. g* (-) groups stained with basic fuchsin and methylene blue (7× and 15× magnification), (b): Images of M, B, HA, and TiN, with *P. g* (+) groups stained with basic fuchsin and methylene blue (7× and 15× magnification), (c): The results of measurement of upside BIC with *P. g* (+), \**P* < 0.05, (d): The results of measurement of downside BIC with *P. g* (-), \**P* < 0.05, (e): The results of measurement of downside BIC with *P. g* (+), \**P* < 0.05.





Despite the surface roughness of TiN, adherence by *P. gingivalis* was difficult. Annunziata *et al.*, (2008) reported that results of three independent experiments showed lower adhesion and proliferation ( $P < 0.05$ ) by *Streptococcus pyogenes* and *S. sanguinis* on TiN-coated TPS surfaces. In addition, TiN surfaces showed a significant reduction of the presence of bacteria, which could be important in decreasing inflammation in peri-implant soft tissues (Scarano *et al.*, 2003). Furthermore, Ji *et al.*, (2015) reported that their in vitro study evaluated antimicrobial activity against not only *S. mutans* but also *P. gingivalis* by TiN-coating on titanium. The results in this study confirmed that TiN exercised antimicrobial activity against *P. gingivalis* both in vivo and in vitro. The results of the upside BIC in the *P. g (+)* group showed the highest percentage for TiN. It was suggested that TiN induced bone formation

and inhibited *P. gingivalis* adhesion, thus preventing inflammation. Moreover, Ji *et al.*, (2015) reported that TiN-coated titanium did not influence osteoblast-like cell viability. However, the downside BIC in the *P. g (+)* group showed almost the same high percentage for B, HA, and TiN. Yuan *et al.*, (2014) reported that BIC with *P. intermedia* infection showed a higher percentage in the implant with a smooth compared to a rough surface. This report conflicted with our results. However, Yuan *et al.*, (2014) used implants completely dipped in bacterial suspension. Our study only used silk threads with a bacterial suspension to infect implants with *P. gingivalis*. The different infection methods may have resulted in different findings between our study and that of them. Furthermore, in the results for the upside BIC, there was only a significant difference between TiN and M, B, and HA. This might

indicate that our experimental period of 2 weeks was sufficient to infect the upside implants. However, future studies using a longer experimental period are needed to evaluate infection of downside implants.

The present study was the first to report that TiN-coated cp titanium implants are excellent as dental implants to induce osseointegration and inhibit *P. gingivalis* infection using a simplified animal model. It is expected that TiN-coated cp titanium implants will be used as dental implants.

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